Cellular Signaling Networks Function as Generalized Wiener-Kolmogorov Filters to Suppress Noise

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Cellular signaling involves the transmission of environmental information through cascades of stochastic biochemical reactions, inevitably introducing noise that compromises signal fidelity. Each stage of the cascade often takes the form of a kinase-phosphatase push-pull network, a basic unit of signaling pathways whose malfunction is linked with a host of cancers. We show that this ubiquitous enzymatic network motif effectively behaves as a Wiener-Kolmogorov optimal noise filter. Using concepts from umbral calculus, we generalize the linear Wiener-Kolmogorov theory, originally introduced in the context of communication and control engineering, to take nonlinear signal transduction and discrete molecule populations into account. This allows us to derive rigorous constraints for efficient noise reduction in this biochemical system. Our mathematical formalism yields bounds on filter performance in cases important to cellular function—such as ultrasensitive response to stimuli. We highlight features of the system relevant for optimizing filter efficiency, encoded in a single, measurable, dimensionless parameter. Our theory, which describes noise control in a large class of signal transduction networks, is also useful both for the design of synthetic biochemical signaling pathways and the manipulation of pathways through experimental probes such as oscillatory input.

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I. INTRODUCTION

Extracting signals from time series corrupted by noise is a challenge in a number of seemingly unrelated areas. Minimizing the effects of noise is a critical consideration in designing communication and navigation systems and analyzing data in diverse fields such as medical and astronomical imaging. More recently, a number of studies have focused on how biological circuits, composed of chemical signaling pathways mediated by genes, proteins, and RNA, cope with noise [1]. One of the key discoveries in the past decade is that the naturally occurring systems that control all aspects of cellular processes undergo substantial stochastic fluctuations in both their expression levels and activities. Noise may even have a functional role [2], providing coordination between multiple interacting chemical partners in typical circuits. Because of the variety of ways noise influences cellular functions, it is important to develop a practical and general theoretical framework for describing how biological systems cope with and control the inevitable presence of noise arising from stochastic fluctuations. In the context of communication theory, the optimal noise-reduction filter, discovered independently by Wiener [3] and Kolmogorov [4] in the 1940s, inaugurated

the modern era of signal processing, providing the first general solution to the problem of extracting useful information from corrupted signals. We show that this classic result of wartime mathematics, developed to guide radarassisted antiaircraft guns, yields insights into the efficiency limits of generic biochemical signaling networks.

Dealing with noise in biological signal transduction is at first glance even more daunting than in engineered systems. In order to survive, cells must process information about their external environment [5-9], which is transmitted and amplified from stimulated receptors on the cell surface through elaborate pathways of post-translational covalent modifications of proteins. A typical example is phosphorylation by protein kinases of target proteins, which then become activated to modify targets further downstream. Signaling occurs through cascades involving multiple stages of such activation [Fig. 1(a)]. Since each enzymatic reaction is stochastic, noise inevitably propagates through the cascade, potentially corrupting the signal [10,11]. Our work focuses on a basic signaling circuit: a "push-pull loop" where a substrate is activated by one enzyme (i.e., phosphorylation by a kinase) and deactivated by another (i.e., dephosphorylation by a phosphatase) [12–15] [Fig. 1(b)]. Since cascades have a modular structure, formed through many such loops in series and parallel, understanding the stochastic properties at the single-loop level is a prerequisite to addressing the complex behavior of entire pathways [16–18].

The push-pull loop can act like an amplifier, taking the input signal—the time-varying population of kinase—and

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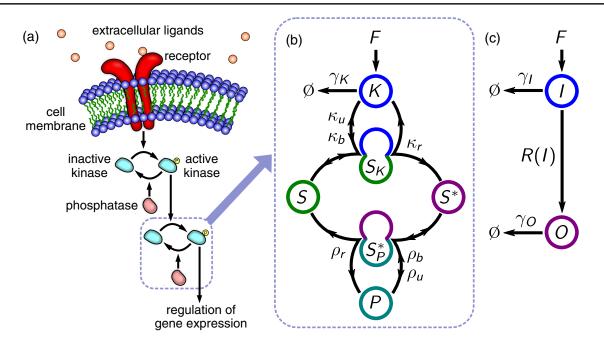


FIG. 1. Schematic of a signaling cascade. (a) A signaling pathway involving cascades of kinase phosphorylation, activated by a receptor embedded in the cell membrane that responds to extracellular ligands. (b) A close-up of one enzymatic push-pull loop within the cascade. Kinase (*K*) phosphorylates the substrate (*S*), converting it to active form (S^*), while phosphatase (*P*) reverts it to the original form through dephosphorylation. S_K and S_P^* represent the substrate in complex with the kinase and phosphatase, respectively. The rate parameters labeling the reaction arrows are described in the text. The input $I = K + S_K$ and output $O = S^* + S_P^*$. (c) A minimal signaling circuit, involving an input species *I* and output species *O*, related by the production rate function R(I).

approximately reproducing it at larger amplitude through the output—the population of active, phosphorylated substrate [14]. Depending on the parameters, small changes in the input can be translated into large (but noise-corrupted) output variations. The amplification is essential for sensitive response to external stimuli, but it must also preserve signal content to be useful for downstream processes. Thus, the signaling circuit, despite operating in a noisy environment, needs to maintain a high fidelity between output and amplified input.

From a design perspective, the natural question that arises is, what are the general constraints on filter efficiency? Are there rigorous bounds, which depend only on certain collective features of the underlying biochemical network architecture? Discovering such bounds is important both to explain the metabolic costs of noise suppression in biological systems [19] and also for bioengineering purposes. In particular, for constructing synthetic signaling networks, we would like to make the most efficient communication pathway with a limited set of resources (free-energy costs).

To answer these questions, using the enzymatic pushpull loop as an example, we introduce a new mathematical framework, inspired by the Wiener-Kolmogorov (WK) theory for optimal noise filtration. The original WK theory has restrictions that make it of limited utility in the biological context—it assumes that the input and output are continuous variables describing stationary stochastic processes. More critically, the filter is assumed to be linear. Exploiting the power of exact analytical techniques based on umbral calculus [20], we overcome these limitations, thus generalizing the WK approach. This crucial theoretical development enables us to provide a rigorous solution to the filter optimization problem, taking into account discrete populations and nonlinearity. We can thus understand constraints in biologically significant regimes of the push-pull loop behavior, for example, highly nonlinear, "ultrasensitive" amplification [13]. Our theory predicts that optimality can be realized by tuning phosphatase levels, which we verify through simulations of a microscopic model of the loop reaction network, including cases where the system is driven by an oscillatory input [21], which is relevant to recent experimental probes [5,6]. The optimality is robust, with the filter operating at near-optimal levels even when the WK conditions are only approximately fulfilled, over a broad range of realistic parameter values. Although illustrated using a push-pull loop, the theory is applicable to a large class of signaling networks, including more complex features such as negative feedback or multisite phosphorylation of substrates.

II. RESULTS AND DISCUSSION

A. Theoretical framework for a minimal signaling circuit

To obtain the central results, we start with an example that illustrates the efficacy of the WK theory and suggests a way to a more detailed, realistic model of the enzymatic push-pull loop. Consider a small portion of a signaling pathway [Fig. 1(c)], involving two chemical species: one with time-varying population I(t) (the "input"), and another one with population O(t) (the "output") whose production depends on I(t). These could be, for example, the active, phosphorylated forms of two kinases within a signaling cascade, with O downstream of I. The upstream part of the pathway contributes an effective production rate F for species I, which, in general, can be time dependent, though for now we will make F constant. The output O is produced by a reaction, $I \xrightarrow{R(I)} I + O$, with a rate R(I(t)) that depends on the input. The species are deactivated with respective rates γ_I and γ_O , mimicking the role of the phosphatases. The input I(t) will vary over a characteristic time scale γ_I^{-1} , fluctuating around the mean $\overline{I} = F/\gamma_I$. The output deactivation rate sets the response time scale γ_0^{-1} over which O(t) can react to changes in the input. The dynamical equations, within a continuum, chemical Langevin (CL) description [22], are given by

$$\frac{dI}{dt} = F - \gamma_I I + n_I, \qquad \frac{dO}{dt} = R(I) - \gamma_O O + n_O, \quad (1)$$

where the additive noise contribution $n_{\alpha}(t) = \sqrt{2\gamma_{\alpha}\bar{\alpha}}\eta_{\alpha}(t)$, with $\alpha = I$, O and $\bar{\alpha}$ denoting the mean of population α . The function $\eta_{\alpha}(t)$ is Gaussian white noise with correlation $\langle \eta_{\alpha}(t)\eta_{\alpha'}(t')\rangle = \delta_{\alpha\alpha'}\delta(t-t')$. The angle brackets denote an average over the ensemble of all possible noise realizations.

For small deviations, $\delta \alpha(t) = \alpha(t) - \bar{\alpha}$, from the mean populations $\bar{\alpha}$, Eq. (1) can be solved using a linear approximation, where we expand the rate function to first order, $R(I(t)) \approx R_0 \bar{I} + R_1 \delta I(t)$, with coefficients R_0 , $R_1 > 0$. (We will return later to the issues of nonlinearity and discrete populations.) The result is

$$\delta I(t) = \int_{-\infty}^{t} dt' e^{-\gamma_{I}(t-t')} n_{I}(t'),$$

$$\delta O(t) = \int_{-\infty}^{t} dt' \frac{R_{1}}{G} e^{-\gamma_{O}(t-t')} \left[G \delta I(t') + \frac{G}{R_{1}} n_{O}(t') \right], \quad (2)$$

where in the second line we introduce an arbitrary scaling factor G > 0 (to be defined below) inside the brackets, and divided through by G outside the brackets. The solution for $\delta O(t)$ has the structure of a linear noise-filter equation: $\tilde{s}(t) = \int_{-\infty}^{t} dt' H(t-t')c(t')$, with c(t) = s(t) + n(t). In this analogy, we have a signal $s(t) \equiv G\delta I(t)$ together with a noise term $n(t) \equiv GR^{-1}n_O(t)$ forming a corrupted signal c(t). The output $\tilde{s}(t) \equiv \delta O(t)$ is produced by convolving c(t) with a linear filter kernel $H(t) \equiv R_1 G^{-1} \exp(-\gamma_O t)$. As a consequence of causality, the integrals in Eq. (2) run over t' < t, so the filtered output $\tilde{s}(t)$ at any time t depends only on c(t') from the past.

The utility of mapping the push-pull system onto a noise filter comes from the application of WK theory, which is designed to solve a key optimization problem: out of all possible causal, linear filters H(t), what is the optimal function $H_{WK}(t)$ that minimizes the differences between the output $\tilde{s}(t)$ and input s(t) time series? In our example, this means having $\delta O(t)$ reproduce as accurately as possible the scaled input signal $G\delta I(t)$. Specifically, we would like to minimize the relative mean-squared error $E = \langle (\tilde{s} - s)^2 \rangle / \langle s^2 \rangle$. For a particular $\delta I(t)$ and $\delta O(t)$, the value of *E* is smallest when $G = \langle (\delta O)^2 \rangle / \langle \delta O \delta I \rangle$, which we use to define the gain *G*. In this case, *E* reduces to $E = 1 - \langle \delta O \delta I \rangle^2 / [\langle (\delta O)^2 \rangle \langle (\delta I)^2 \rangle]$. The great achievement of Wiener [3] and Kolmogorov [4] was to show that H_{WK} satisfies the following Wiener-Hopf equation:

$$C_{cs}(t) = \int_{-\infty}^{t} dt' H_{WK}(t-t') C_{cc}(t'), \quad t > 0, \quad (3)$$

where $C_{xy}(t) \equiv \langle x(t')y(t'+t) \rangle$ is the correlation between points in time series x and y, assumed to depend only on the time difference t. Given C_{cs} and C_{cc} , which are properties of the signal s(t) and noise n(t), it is possible to solve Eq. (3) for H_{WK} . The corresponding minimum value of the error E is

$$E_{\rm WK} = 1 - \frac{1}{C_{ss}(0)} \int_0^\infty dt H_{\rm WK}(t) C_{cs}(t).$$
(4)

The solution of the Wiener-Hopf equation requires the following correlation functions, which can be derived from Eq. (2): $C_{ss}(t) = C_{cs}(t) = G^2 \overline{I} \exp(-\gamma_I |t|)$, $C_{nn}(t) = 2G^2 \overline{I} \delta(t)/(\gamma_I \Lambda)$, and $C_{cc}(t) = C_{ss}(t) + C_{nn}(t)$, where the parameter $\Lambda \equiv R_1^2/(R_0\gamma_I)$. Plugging these into Eq. (3), we can solve for the optimal filter function by assuming a generic ansatz $H_{WK}(t) = \sum_{i=1}^N A_i \exp(-\lambda_i t)$, finding the unknown coefficients A_i and rate constants λ_i by comparing the left-hand and right-hand sides of the equation. In our case, a single exponential (N = 1) is sufficient to exactly satisfy Eq. (3) (see details in Appendix A), and we get $H_{WK}(t) = \gamma_I(\sqrt{1 + \Lambda} - 1) \exp(-\gamma_I\sqrt{1 + \Lambda}t)$. The conditions for achieving WK optimality, $H(t) = H_{WK}(t)$, are then

$$\gamma_O = \gamma_I \sqrt{1 + \Lambda}, \qquad G = \frac{R_1}{\gamma_I (\sqrt{1 + \Lambda} - 1)}.$$
 (5)

From Eq. (4), the minimum relative error is

$$E_{\rm WK} = \frac{2}{1 + \sqrt{1 + \Lambda}}.\tag{6}$$

The fidelity between output and input is described through a single dimensionless optimality control parameter Λ . It can be broken up into two multiplicative factors, reflecting two physical contributions: $\Lambda = (R_0/\gamma_I)(R_1/R_0)^2$. The first term, R_0/γ_I , is a burst factor, measuring the mean number of output molecules produced per input molecule during the active lifetime of the input molecule. The second term, $(R_1/R_0)^2$, is a sensitivity factor, reflecting the local response of the production function R(I) near \overline{I} [controlled by the slope $R_1 = R'(\bar{I})$ relative to the production rate per input molecule: $R_0 = R(\bar{I})/\bar{I}$. Note that $(R_1/R_0)^2 > 1$ only if R(I) is globally nonlinear, since physical production functions satisfy $R(I) \ge 0$ for all $I \ge 0$. If R(I) is perfectly linear, $R(I) = R_0 I$, then $R_1 = R_0$, and $(R_1/R_0)^2 = 1$. Thus, the limit of efficient noise suppression, $\Lambda \gg 1$, where $E_{\rm WK}$ becomes small, can be achieved by making the burst factor $R_0/\gamma_I \gg 1$ and/or enhancing the sensitivity $(R_1/R_0)^2 \gg 1$, at the cost of introducing nonlinear effects (discussed in detail below). For optimality to be realized, we additionally need an appropriate separation of scales [Eq. (5)] between the characteristic time of variations in the input signal γ_I^{-1} and the response time of the output γ_Q^{-1} . The latter should be faster by a factor of $\sqrt{1+\Lambda}$. The scaling $E_{\rm WK} \sim \Lambda^{-1/2}$ for large Λ is the same as the burstfactor scaling of the target population variance in biochemical negative feedback networks intended to maintain homeostasis and suppress fluctuations [19]. The slow $\Lambda^{-1/2}$ decay in both cases, compared to the more typical scaling of variance with Λ^{-1} (inversely proportional to the number of signaling molecules produced), reflects the same underlying physical challenge: the difficulty of suppressing or filtering noise in stochastic reaction networks.

The error *E* defined above is based on the instantaneous difference between the input s(t) and output $\tilde{s}(t)$ time series. One of the powerful features of the WK formalism is that it naturally extends error minimization to cases where the goal is extrapolating the future signal, where we seek to minimize the difference between $\tilde{s}(t)$ and $s(t + \alpha)$ for some $\alpha > 0$ [23]. Given the time delays inherent in many biological responses, particularly, where feedback is involved, such predictive noise filtering has significant applications [24], which we will explore in subsequent work. For now, we confine ourselves to the instantaneous error, which is sufficient to treat the kinase-phosphatase push-pull loop.

We also note that there is no unique measure of signal fidelity. Besides E, one can optimize the mutual information between the output and input species in the cascade [17]. For example, in the two-component cascade with nonlinear regulation, considered below, a spectral expansion of the master equation allows for efficient numerical optimization of the system parameters for particular forms of the rate function, maximizing the mutual information [25,26].

B. Effects of nonlinearity and discrete populations

For the subclass of Gaussian-distributed signal s(t) and noise n(t) time series (as is the case within the CL picture),

the WK filter derived above, based on the linearization of the CL, is optimal among all possible linear or nonlinear filters [23]. If the system fluctuates around a single stable state, and the copy numbers of the species are large enough that their Poisson distributions converge to Gaussians (mean populations \gtrsim 10), the signal and noise are usually approximately Gaussian. However, the rate function R(I)will never be perfectly linear in practice, and thus, one needs to consider how nonlinearities in R(I) will affect the minimal E. In addition, the discrete nature of population changes, which becomes important at lower copy numbers, has to be explicitly taken into consideration. Surprisingly, the WK result of Eq. (6) can be generalized even to cases where the linear, continuum assumptions underlying WK theory no longer hold.

Starting from the exact master equation, valid for discrete populations and arbitrary R(I), we rigorously solve the general optimization problem for the error E between output and input using the principles of umbral calculus [20]. The detailed proof is in Appendix B, but the main results are as follows. Any function R(I) can be expanded in terms of a set of polynomials $v_n(I)$ as $R(I) = \sum_{n=0}^{\infty} \sigma_n v_n(I)$. The $v_n(I)$ are polynomials of degree n, given by

$$v_n(I) = \sum_{m=0}^n (n-m)! (-\bar{I})^m \binom{n}{m} \binom{I}{n-m}, \quad (7)$$

and the coefficients σ_n are related to moments of R(I), $\sigma_n = \langle v_n(I)R(I) \rangle / (\bar{I}^n n!)$. The average is taken with respect to the Poisson distribution $\mathcal{P}(I) = \bar{I}^I \exp(-\bar{I})/I!$. The first two polynomials are $v_0 = 1$ and $v_1 = I - \bar{I}$, giving $\sigma_0 = \langle R(I) \rangle$ and $\sigma_1 = \langle (I - \bar{I})R(I) \rangle / \bar{I}$. Remarkably, the relative error *E* has an exact analytical form in terms of the σ_n ,

$$E = 1 - \frac{\bar{I}\gamma_O^2 \sigma_1^2}{(\gamma_I + \gamma_O)^2} \left[\gamma_O \sigma_0 + \sum_{n=1}^{\infty} \sigma_n^2 \frac{\gamma_O n! \bar{I}^n}{\gamma_O + n\gamma_I} \right]^{-1}.$$
 (8)

This expression is bounded from below by

$$E \ge E_{\text{opt}} \equiv \frac{2}{1 + \sqrt{1 + \tilde{\Lambda}}},\tag{9}$$

where $\tilde{\Lambda} = \bar{I}\sigma_1^2/(\sigma_0\gamma_I)$. The equality is reached only when $\gamma_O = \gamma_I \sqrt{1 + \tilde{\Lambda}}$ and R(I) has an optimal linear form, $R_{\text{opt}}(I) = \sigma_0 + \sigma_1(I - \bar{I})$, with all $\sigma_n = 0$ for $n \ge 2$. In this optimal case, $\sigma_0 = R_0\bar{I}$ and $\sigma_1 = R_1$, and hence, $\tilde{\Lambda} = \Lambda$, $E = E_{\text{opt}} = E_{\text{WK}}$ from Eq. (6).

Making Λ large, for example, by increasing σ_1 , is desirable for better signal transduction, but with a caveat. We can keep *E* near E_{opt} even for a globally nonlinear R(I) so long as R(I) remains approximately linear in the vicinity

of the mean \overline{I} , and the nonlinear corrections σ_n for $n \ge 2$ are negligible. Large σ_1 can be achieved through a highly sigmoidal input-output response, known as ultrasensitivity, which is biologically realizable in certain regimes of signaling cascades [13]. However, our theory predicts that as R(I) goes to the extreme limit of a steplike profile around \overline{I} , E should become significantly higher than E_{opt} , and the benefits of ultrasensitivity vanish. The reason for this is that letting σ_1 become arbitrarily large (making the step sharper) necessarily implies that R(I) eventually deviates substantially from $R_{opt}(I)$. We know that any physically sensible R(I) satisfies the constraint $R(I) \ge 0$ for $I \ge 0$. If $\sigma_1 \gg \sigma_0/\overline{I}$ and $\sigma_n \approx 0$ for $n \ge 2$, the function R(I) would be negative for $I \leq \overline{I} - \sigma_0/\sigma_1$, violating the physical constraint. Hence, the coefficients σ_n for $n \ge 2$ must be non-negligible when σ_1 is sufficiently large, leading to $E > E_{opt}$.

We can illustrate this result numerically for R(I) that have the form of a Hill function, $R(I) = R_s(I/I_0)^{n_H}/$ $[1 + (I/I_0)^{n_H}]$, defined by the three parameters R_s , I_0 , and n_H . This represents a typical sigmoidal behavior in biochemical systems, with a small production rate for $I \ll I_0$ switching over to a saturation level R_s for $I \gg I_0$. We perform a numerical minimization of E [evaluated using Eq. (8)] over the parameter space, at fixed F, γ_I , σ_0 , and Λ . Using Eq. (8) is numerically extremely efficient, since the coefficients σ_n typically decay quite rapidly, allowing the infinite sum to converge after a small (less than 10) number of terms. Fixing σ_0 and Λ is equivalent to specifying the first two moments of R(I), which in turn defines a curve in the three-dimensional parameter space of R_s , I_0 , and n_H . After numerically solving for this curve, the minimization procedure consists of searching along the curve (and varying the free system parameter γ_0) to find the parameter set that yields the smallest E. Figure 2(a) shows optimization results for $F = 1 \text{ s}^{-1}$, $\gamma_I = 0.01 \text{ s}^{-1}$, $\sigma_0 = 100 \text{ s}^{-1}$, and varying Λ , with the optimal Hill function R(I) (the one with smallest E) at each Λ drawn in a different color. The corresponding minimal values of Eare shown in Fig. 2(b) as circles in the same colors, with E_{opt} using Eq. (9) drawn as a blue curve for comparison. Larger values of $\tilde{\Lambda}$ have optimal R(I) profiles that are increasingly steplike, with steeper slopes near \overline{I} . For the range $\Lambda = 10^2 - 10^3$, the maximum slope ($\approx \sigma_1$) is still small enough that R(I) remains approximately linear across the entire I range, where $\mathcal{P}(I)$ is non-negligible [the distribution is superimposed in Fig. 2(a)]. Hence, minimal E values are very close to E_{opt} , decreasing with Λ . The ratios γ_O/γ_I at which these minimal E values occur, shown in Fig. 2(c), are nearly equal to the predicted value $\sqrt{1+\Lambda}$ (blue curve). We can estimate that this near optimality will persist up to $\sigma_1 \approx \sigma_0/(3\sqrt{I})$, since that is roughly the slope of an R(I) that rises from zero near the left edge of $\mathcal{P}(I)$ (at

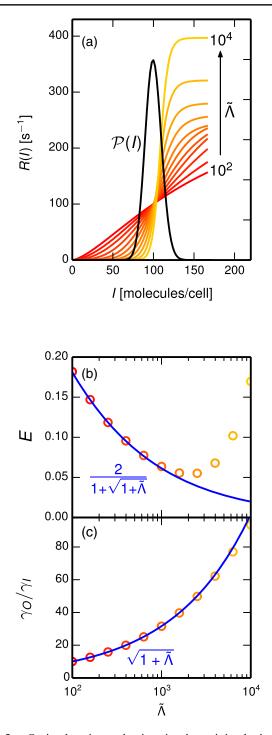


FIG. 2. Optimal noise reduction in the minimal signaling circuit [Fig. 1(c)]. (a) Numerical optimization results for the Hill production function R(I) that minimizes relative error E between input and output, with each color corresponding to different values of the parameter $\tilde{\Lambda} = 10^2 - 10^4$ (see text for other parameters). The input probability distribution $\mathcal{P}(I)$ is super-imposed in black (the height scale is arbitrary). (b) For each value of $\tilde{\Lambda}$ from (a), circles show the minimal E. The lower bound E_{opt} [Eq. (9)] is drawn as a blue curve. (c) Analogous to (b), but showing the ratio γ_O/γ_I at which the minimum E is achieved. The blue <u>curve</u> shows the WK prediction for this ratio, $\gamma_O/\gamma_I = \sqrt{1 + \tilde{\Lambda}}$.

 $I \approx \overline{I} - 3\sqrt{\overline{I}}$ to a value of σ_0 at $I = \overline{I}$. For $\sigma_1 \gtrsim \sigma_0/(3\sqrt{\overline{I}})$, or equivalently $\tilde{\Lambda} \gtrsim \sigma_0/(9\gamma_I) = 1.1 \times 10^3$, the nonlinearity of R(I) becomes appreciable around \overline{I} , distorting the output signal and leading to minimal E noticeably larger than E_{opt} , and actually increasing with $\tilde{\Lambda}$. Thus, moving toward the ultrasensitive limit $\tilde{\Lambda} \to \infty$ is initially beneficial for noise filtering, but only up to a point: R(I) does not have to be globally linear, but local linearity of R(I) near \overline{I} , which can be satisfied readily, is best for accurate signal transduction.

C. Enzymatic push-pull loop acts as an optimal WK filter

The system considered so far is the simplest realization of a signaling circuit, in the sense that it involves only two species, related through a single phenomenological production function R(I). In reality, an enzymatic pushpull loop involves intermediates—complexes of the substrate with the kinase or phosphatase—whose binding, unbinding, and catalytic reactions all contribute to the stochastic nature of signal transmission. Can the WK theoretical framework be used to describe optimality in this complicated context? Let us consider a more microscopic model of the loop reaction network [Fig. 1(b)]. The active kinase is either free (K) or bound to substrate (S_K). The input I is defined as the total active kinase population $I = K + S_K$. Upstream modules control kinase activation and deactivation, described by rates F and γ_K , respectively. The kinase can phosphorylate the substrate, converting it from inactive (S) to active (S^{*}) form. Analogously, in the reverse direction, free phosphatases (P) form complexes with the active substrate (S_P^*), which lead to dephosphorylation, returning the substrate to inactive form. The output O is the total active substrate population $O = S^* + S_P^*$. The reactions for substrate modification, with corresponding rate constants, are

$$K + S \underset{\kappa_u}{\stackrel{\kappa_b}{\longleftrightarrow}} S_K \overset{\kappa_r}{\xrightarrow{}} K + S^*,$$

$$P + S^* \underset{\rho_u}{\stackrel{\rho_b}{\longrightarrow}} S_P^* \overset{\rho_r}{\xrightarrow{}} P + S.$$
 (10)

We choose representative rate values based on a model of the mitogen-activated protein kinase cascade [27] (all units are in s⁻¹): $\kappa_b = \rho_b = 10^{-5}$, $\kappa_u = 0.02$, $\rho_u = 0.5$, $\kappa_r = 3$, $\rho_r = 0.3$, F = 1. The rate γ_K in the model controls the characteristic time scale over which the input signal varies. We let $\gamma_K = 0.01 \text{ s}^{-1}$, which sets this scale to minutes. Mean free substrate and phosphatase populations (which together with the rates determine all equilibrium population values) are in the ranges $\bar{S} \sim 10^4 - 10^5$, $\bar{P} \sim 10^3 - 10^6$ molecules/cell.

We simulate the dynamics of this system numerically using the kinetic Monte Carlo (KMC) method [28], with sample input and output trajectories shown in Figs. 3(d)– 3(f) for $\bar{S} = 8 \times 10^4$ and three values of \bar{P} . As the free

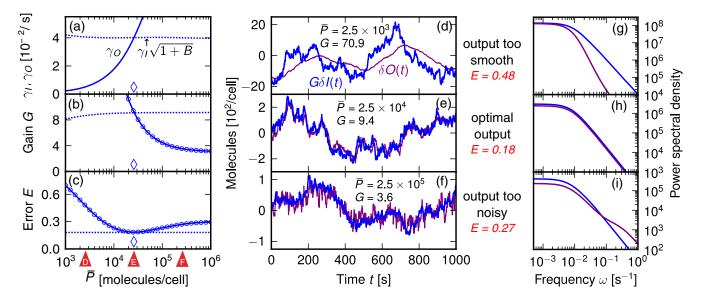


FIG. 3. (a) γ_O (solid curve) and $\gamma_I \sqrt{1 + \Lambda}$ (dashed curves), based on the mapping in Eq. (11), for $\Lambda = 100$. The \bar{P} value at the intersection of the solid and dashed curves, where the WK optimality conditions are fulfilled, is indicated by a diamond. (b) Gain *G* (solid line, CL theory; circles, KMC simulations) for the same Λ value as in (a), versus the WK optimal value for *G* (dashed line) given by Eq. (5). (c) Same as (b), but showing error *E* versus the WK optimal prediction E_{WK} (dashed line) from Eq. (6). (d)–(f) Sample trajectories for the scaled input $G\delta I(t)$ (blue curve) and the output $\delta O(t)$ (purple curve) from KMC simulations of the push-pull loop, for $\Lambda = 100$ ($\bar{S} = 8 \times 10^4$) and three different values of \bar{P} . These \bar{P} values are marked by red triangles under (c) and correspond to cases where, relative to the input, the output is too smooth (d), optimal (e), and too noisy (f). (g)–(i) Power spectral densities of the scaled input $G\delta I(t)$ (blue curve) for the three cases shown in (d)–(f).

phosphatase population is varied, we see different degrees of signal fidelity, with the closest match between $\delta O(t)$ and $G\delta I(t)$ for the intermediate case in Fig. 3(e). Are we seeing behavior similar to an optimal WK filter? As detailed in Appendix C, we can approximately map the phosphorylation cycle to a noise filter using the same method as in our first example: starting from the full dynamical equations in the linear CL approximation, we derive the correlation functions required to solve the Wiener-Hopf relation, Eq. (3). The effective parameters resulting from the mapping are

$$\gamma_{O} = \frac{\rho_{r}\rho_{+}}{\sqrt{\rho^{2} - 2\rho_{r}\rho_{+}}}, \qquad R_{1} = \frac{\kappa_{r}\kappa_{+}\rho}{\kappa\sqrt{\rho^{2} - 2\rho_{r}\rho_{+}}},$$
$$\gamma_{I} = \frac{\kappa_{-}\gamma_{K}}{\kappa}, \qquad \Lambda = \frac{\kappa_{r}\kappa_{+}\kappa^{2}\rho^{2}}{\gamma_{K}\kappa_{-}[\rho^{2}(\kappa^{2} - \kappa_{r}\kappa_{+}) - \rho_{r}\rho_{+}\kappa^{2}]}, \quad (11)$$

where $\kappa_{+} = \kappa_{b}\bar{S}$, $\kappa_{-} = \kappa_{u} + \kappa_{r}$, $\kappa = \kappa_{+} + \kappa_{-}$, $\rho_{+} = \rho_{b}\bar{P}$, $\rho_{-} = \rho_{u} + \rho_{r}$, and $\rho = \rho_{+} + \rho_{-}$. Equation (11) is valid in the regime $\bar{K} = F/\gamma_K \ll \bar{S}$, \bar{P} , with corrections of order $\overline{K}/\overline{S}$ and $\overline{K}/\overline{P}$ shown in Appendix C. Such a mapping allows us to use WK results in Eqs. (5) and (6) to predict the conditions for optimality and the minimal possible E. Figures 3(a) and 3(b) show the left-hand (solid lines) and right-hand (dashed lines) sides of both conditions in Eq. (5) as a function of \bar{P} for $\Lambda = 100 \ (\bar{S} = 8 \times 10^4)$. The \bar{P} value at the intersections, where the conditions are fulfilled, is marked by a diamond. Figure 3(c) shows that exactly at this value E achieves a minimum, given by E_{WK} from Eq. (6) (dashed line). The CL approximation (solid curves) and KMC simulations (circles) are in excellent agreement. Thus, the phosphorylation cycle can indeed be tuned to behave like an optimal WK noise filter, even for a realistic signaling model. In light of the mapping in Eq. (11), we now understand the behavior of the trajectories in Fig. 3(d)–3(f), which correspond to $\Lambda = 100$. In Fig. 3(d), where $\bar{P} = 2.5 \times 10^3$, we have $\gamma_O \ll \gamma_I \sqrt{1 + \Lambda}$ [Fig. 3(a)], and the output $\delta O(t)$ becomes excessively smooth, since it cannot respond quickly enough to changes in the input signal $G\delta I(t)$. The corresponding power spectral density (PSD) of the output, shown in Fig. 3(g), is smaller at high frequencies compared to the PSD of the input. In Fig. 3(f), we have the opposite situation of $\gamma_O \gg \gamma_I \sqrt{1 + \Lambda}$ at $\bar{P} = 2.5 \times 10^5$. The output response is too rapid, generating additional noise that obscures the signal. In this case, the output PSD [Fig. 3(i)] has an extra high-frequency contribution relative to the input PSD. Figure 3(e) represents the optimal intermediate $\bar{P} = 2.5 \times 10^4$, where $\gamma_0 =$ $\gamma_I \sqrt{1 + \Lambda}$ and the WK conditions are fulfilled. The input and output PSDs [Fig. 3(h)] are similar at all frequencies.

The minimum of E in Fig. 3(c) is shallow, meaning that near-optimal filtering persists even when the phosphatase population is not precisely tuned to the WK condition. For \overline{P} values that vary nearly fivefold between

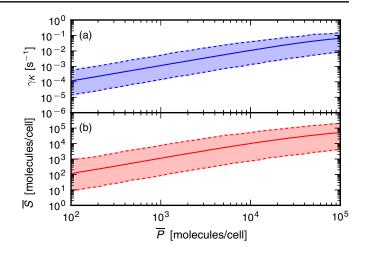


FIG. 4. Conditions for WK optimality as the enzymatic pushpull loop parameters are varied. (a) The solid blue curve shows the relation between mean phosphatase population \bar{P} and the characteristic frequency scale γ_K over which the active kinase input signal varies. This is at WK optimality [Eq. (5)], using the mapping of Eq. (11) and the parameter values κ_b , ρ_b , κ_u , ρ_u , κ_r , ρ_r listed in the text after Eq. (10). The shaded region between the dashed curves shows the 68% confidence interval for achieving WK optimality, resulting from randomly perturbing all the parameter values so that they can be up to tenfold smaller or larger. (b) Analogous to (a), but showing the relation between \bar{P} and substrate population \bar{S} at WK optimality.

 $\overline{P} = (1.3-6.3) \times 10^4$, the error E remains within 5% of the minimum value $E_{\rm WK}$. Another aspect of the filter's robustness can be highlighted by perturbing the enzymatic parameters κ_b , ρ_b , κ_u , ρ_u , κ_r , and ρ_r . If we randomly vary all these parameters within a range between 0.1 and 10 times the values listed above after Eq. (10), and calculate the resulting conditions for WK optimality [Eq. (5)] for each new parameter set, we obtain the results in Fig. 4. For a given \bar{P} , the shaded intervals in the figure correspond to the 68% confidence intervals on the input kinase frequency scale γ_K and the mean substrate population \bar{S} at optimality. Thus, for a broad range of biologically relevant enzymatic parameters, we get a sense of how the populations of \bar{P} and \overline{S} must complement each other and an associated time scale γ_{K}^{-1} reflecting how quickly the input signal can vary and still be accurately transduced. From the trends in Fig. 4, we see that to get the system to respond to more rapidly varying signals, we need larger populations of \overline{P} and \overline{S} . As a concrete example, for the hyperosmolar glycerol (HOG) signaling pathway in yeast, which we discuss in the next section, kinase substrates have cell copy numbers of between 6×10^1 and 7×10^3 , while the tyrosine protein and type 2C protein phosphatases that have been identified as targeting the pathway are present in cell copy numbers between 1.5×10^2 and 2×10^4 [29]. Using these population scales as a rough guide for \bar{S} and \bar{P} (ignoring complications such as multiple phosphorylation steps and sharing of phosphatases between different pathways),

we see from Fig. 4 that the corresponding $\gamma_K \sim 10^{-4} - 10^{-2} \text{ s}^{-1}$. This range of optimal time scales is consistent with the experimental observation that the HOG pathway can faithfully transduce osmolyte signals at frequencies $\lesssim 5 \times 10^{-3} \text{ s}^{-1}$ [5].

D. Noise filtration in a push-pull loop driven by oscillatory input

Remarkably, since Eq. (11) is independent of F, the system can serve as an optimal filter for a range of F values,

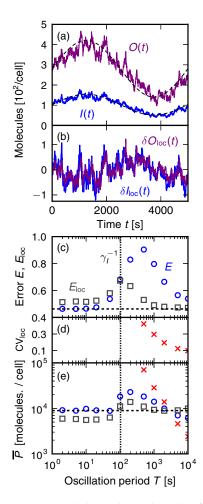


FIG. 5. (a) Sample KMC simulation trajectories for I(t) (solid blue) and O(t) (solid purple) in a $\Lambda = 10$ system driven by an oscillatory upstream flux F(t) (see text for parameters). Dashed lines are local means $I_{\rm loc}(t)$ and $O_{\rm loc}(t)$. (b) For trajectories in (a), the deviations from local means, $\delta I_{\rm loc}(t)$ (blue) and $\delta O_{\rm loc}(t)$ (purple). (c)–(e) Results calculated from KMC simulations for a system with $\Lambda = 10$ and oscillatory F(t) at varying driving periods T. γ_I^{-1} is marked by a vertical dashed line. (c) The minimum errors E (circles) and $E_{\rm loc}$ (squares). $E_{\rm WK}$ is marked by a horizontal dashed line. (d) The minimum local coefficient of variation $CV_{\rm loc} = \sqrt{\langle (\delta O_{\rm loc}/\bar{O}_{\rm loc})^2 \rangle}$. (e) The mean phosphatase population values \bar{P} at which the minima shown in (c) and (d) are achieved (E, circles; $E_{\rm loc}$, squares; $CV_{\rm loc}$, crosses). The \bar{P} value for WK optimality is marked by a horizontal dashed line.

so long as the condition $F/\gamma_K \ll \overline{S}$, \overline{P} is satisfied. This regime, involving saturated kinases and unsaturated phosphatases, has previously been identified as a candidate for efficient signal transmission by Gomez-Uribe et al. [18]. To check the filter operation with varying upstream flux, we used a time-dependent F(t), driving the system with oscillatory input. This is motivated by microfluidic experimental setups [5,6], where the HOG pathway of yeast was probed by exposing the cells to periodic osmolyte pulses. In the experiments, the input signal is the extracellular osmolyte concentration and the output is the degree to which the activated kinase Hog1 localizes in the nucleus, where it initiates a transcriptional response to the osmolar shock. Though the biochemical network relating the output to input consists of a complex series of enzymatic push-pull loops, the overall behavior is quantified through response functions in terms of input signal frequency [5], related to the Fourier transforms of the input-output correlation functions. Such correlation functions are the basic ingredients in assessing filter optimality in the WK theory. Here, we focus only on a single push-pull loop and use input at varying frequencies to determine whether E_{WK} remains a meaningful constraint on filter performance even for nonstationary signals. In Fig. 5(a), we show a sample I(t) and O(t) KMC trajectory at optimality for $F(t) = \bar{F}[1 + A\sin(2\pi t/T)]$, with $\bar{F} = 1 \text{ s}^{-1}$, A = 0.5, and T = 5000 s. The input has two characteristic time scales, T and $\gamma_I^{-1} = 10^2$ s. For $T \gg \gamma_I^{-1}$, we define relative error in terms of deviations from local, time-dependent means: E_{loc} defined using $\delta I_{\rm loc} = I(t) - \bar{I}_{\rm loc}(t)$ and $\delta O_{\rm loc} = O(t) - \bar{O}_{\rm loc}(t)$ [Fig. 5(b)], where $\bar{I}_{loc}(t) = \bar{I}F(t)/\bar{F}$, $\bar{O}_{loc}(t) = \bar{O}F(t)/\bar{F}$ are shown as dashed curves in Fig. 5(a). Figure 5(c) shows KMC results for minimum E and minimum E_{loc} as a function of T for a system tuned to optimality with $\Lambda = 10$. The values of \overline{P} at which these minima are achieved are shown in Fig. 5(e). At $T > \gamma_I^{-1}$, we find $E_{\text{loc}} < E$, since both the input and output have time to adjust to the slowly varying local means. In fact, the minimum E_{loc} approaches $E_{\rm WK}$ for $T \gg \gamma_I^{-1}$, as optimality is unaffected by the slow oscillation in F(t). The \bar{P} where the minimum E_{loc} occurs also approaches the value predicted by WK theory [Fig. 5(e)]. The filter transduces the signal with high fidelity. In the opposite limit of small $T < \gamma_I^{-1}$, the rapidly varying F(t) essentially averages out, since neither the input nor the output have time to respond to the sharp changes in F(t). Thus, the system sees an effective constant flux \overline{F} . Here, E, the error estimate with respect to the global mean, is more relevant than E_{loc} . In this regime, the minimum $E < E_{loc}$, E approaches E_{WK} for $T \ll \gamma_I^{-1}$, and the \overline{P} value where E is minimized agrees with the WK prediction.

The two regimes in system behavior, with a changeover at the time scale γ_I^{-1} , reflect the fact that the enzymatic loop acts as an effective low-pass filter [6,14]: it can accurately transmit the low-frequency component of F(t), but integrates over the high-frequency portion above a certain bandwidth. The overall bandwidth of a cascade of pushpull loops has been experimentally characterized for the yeast HOG pathway, yielding a value of $\omega_b \approx 5 \times 10^{-3} \text{ s}^{-1}$ [6]. Using this as a rough estimate of the bandwidth scale γ_I in individual loops, we could expect to see a changeover between the two regimes depending on whether the driving frequency is much slower or faster than ω_b . Regardless of the magnitude of the driving frequency, both *E* and E_{loc} always remain greater than E_{WK} , so the latter remains a bound on noise-filter efficiency even for dynamic input.

More generally, the low-pass filtering property of the enzymatic loop can be fine-tuned to optimize other signal transmission characteristics besides E and E_{loc} . These two errors are minimized when the output fluctuations (δO or $\delta O_{\rm loc}$) closely follow the scaled input fluctuations ($G\delta I$ or $G\delta I_{\rm loc}$). However, one could imagine biological scenarios where the desired outcome was a smoothed output that mirrored the oscillatory driving signal. In other words, we could demand that O(t), as shown, for example, in Fig. 5(a) (purple trajectory), deviates minimally from the oscillatory local mean $\bar{O}_{loc}(t)$ (superimposed dashed line). In this case, the natural quantity to minimize would be a local coefficient of variation, $CV_{loc} = \sqrt{\langle (\delta O_{loc}/\bar{O}_{loc})^2 \rangle}$. From the oscillatory KMC simulations described above, we calculate CV_{loc} , and find that it can be made small in the slow oscillation regime $T \gg \gamma_I^{-1}$, as shown in Fig. 5(d), which plots the minimum CV_{loc} as a function of T for $T \ge 500$ s. From Fig. 5(e), which shows the \overline{P} values at which the minimum CV_{loc} occurs (crosses), we see that in the large T limit this \overline{P} value is smaller than the WK prediction. This makes sense, since as we know from the case of a constant driving function $(T \to \infty)$, illustrated in Fig. 3(d), that keeping \bar{P} below the WK optimum smooths the output. For systems more complex than the enzymatic loop, smoothed output (homeostasis around a constant mean, or tracking of a driven, time-varying local mean) can be enhanced by introducing some negative feedback mechanism from the output back to the input [19]. For such negative feedback systems, it turns out that there exists a mapping onto a different WK filter [30].

III. CONCLUSIONS

We demonstrate the usefulness of a generalized WK filter theory as a way of characterizing signal fidelity in an enzymatic push-pull loop. This basic motif of biological signal transduction can effectively realize an optimal WK noise filter. Through a novel analytical approach, we generalize WK ideas beyond their original linear context, thus providing fidelity bounds in strongly nonlinear cases, including ultrasensitive production and oscillatory input driving. Even for a complex kinase-phosphatase reaction network with multiple intermediates, the theory predicts the conditions for accurate signal transduction, yielding a bound on the error in terms of a single dimensionless optimality control parameter Λ . The results highlight how physics and engineering concepts can be use to understand how biology robustly tunes push-pull loops to optimality by setting the copy numbers of phosphatase and substrate molecules. We can relate the wide range of cellular signaling protein copy numbers observed experimentally to optimal time scales on which the cell can accurately transduce the signal, and thus yield an effective physiological response. Since our approach is formulated in terms of correlation functions of signal and noise, quantities readily accessible from both theory and simulation, the current work can be generalized to other complex signaling networks. The ultimate goal is to give insights into the design principles underlying the large, intertwined biochemical pathways that determine how the cell can process and respond to diverse sources of external stimuli.

ACKNOWLEDGMENTS

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APPENDIX A: SOLVING THE WIENER-HOPF EQUATION FOR THE OPTIMAL FILTER

Given the correlation functions,

$$C_{ss}(t) = C_{cs}(t) = G^2 \overline{I} e^{-\gamma_I |t|}, \qquad C_{nn}(t) = \frac{2G^2 I}{\gamma_I \Lambda} \delta(t),$$

$$C_{cc}(t) = C_{ss}(t) + C_{nn}(t), \qquad (A1)$$

we would like to find the optimal filter function $H_{WK}(t)$ that satisfies the Wiener-Hopf equation,

$$C_{cs}(t) = \int_{-\infty}^{t} dt' H_{WK}(t-t') C_{cc}(t'), \quad t > 0.$$
 (A2)

Since $C_{cs}(t)$ and $C_{cc}(t)$ consist of exponential terms and Dirac delta functions, a reasonable ansatz for $H_{WK}(t)$ is a sum of *N* exponentials, $H_{WK}(t) = \sum_{i=1}^{N} A_i \exp(-\lambda_i t)$, with parameters $A_i, \lambda_i, i = 1, ..., N$. Plugging this into Eq. (A2), along with the correlation functions from Eq. (A1), and carrying out the integral, we find

$$G^{2}\overline{I}e^{-\gamma_{I}t} = \sum_{i=1}^{N} A_{i} \left[\left(\frac{2G^{2}\overline{I}\gamma_{I}}{\gamma_{I}^{2} - \lambda_{i}^{2}} + \frac{2G^{2}\overline{I}}{\gamma_{I}\Lambda} \right) e^{-\lambda_{i}t} + \frac{G^{2}\overline{I}}{\lambda_{i} - \gamma_{I}} e^{-\gamma_{I}t} \right], \quad t > 0.$$
(A3)

Comparing the left-hand and right-hand sides of Eq. (A3), we see that the coefficients of the linearly independent exponential terms on both sides must match, giving N + 1 equations: N coefficients of $\exp(-\lambda_i t)$, plus one for $\exp(-\gamma_I t)$. Since there are 2N unknown parameters in the ansatz, the only value of N that gives a closed set of

equations is N = 1. With this choice of N, the resulting two equations are

$$0 = A_1 \left(\frac{2G^2 \bar{I} \gamma_I}{\gamma_I^2 - \lambda_1^2} + \frac{2G^2 \bar{I}}{\gamma_I \Lambda} \right), \qquad G^2 \bar{I} = \frac{A_1 G^2 \bar{I}}{\lambda_1 - \gamma_I}.$$
 (A4)

The only physically sensible solution of Eq. (A4) for A_1 and λ_1 [where $|H_{WK}(t)| \neq \infty$ as $t \to \infty$] is

$$A_1 = \gamma_I \left(\sqrt{1+\Lambda} - 1 \right), \qquad \lambda_1 = \gamma_I \sqrt{1+\Lambda}.$$
 (A5)

Thus, the optimal filter is

$$H_{\rm WK}(t) = \gamma_I \left(\sqrt{1+\Lambda} - 1\right) e^{-\gamma_I \sqrt{1+\Lambda}t}.$$
 (A6)

APPENDIX B: OPTIMAL SIGNAL TRANSDUCTION FOR THE NONLINEAR, DISCRETE CASE

To obtain results for the general signal pathway model, where we assume neither linearity of the production function R(I) nor a continuum description, we start with an exact equation for the stationary joint distribution $\mathcal{P}(I, O)$ of the input and output. Using this, we will derive expressions for various moments of the distribution that enter into the relative mean-squared error

$$E = 1 - \frac{\langle \delta O \delta I \rangle^2}{\langle (\delta O)^2 \rangle \langle (\delta I)^2 \rangle}$$

= $1 - \frac{(\langle O I \rangle - \langle O \rangle \langle I \rangle)^2}{(\langle O^2 \rangle - \langle O \rangle^2)(\langle I^2 \rangle - \langle I \rangle^2)}.$ (B1)

From the master equation, $\mathcal{P}(I, O)$ satisfies

$$\gamma_{I}[(I+1)\mathcal{P}(I+1,O) - I\mathcal{P}(I,O)] + F[\mathcal{P}(I-1,O) - \mathcal{P}(I,O)] + \gamma_{O}[(O+1)\mathcal{P}(I,O+1) - O\mathcal{P}(I,O)] + R(I)[\mathcal{P}(I,O-1) - \mathcal{P}(I,O)] = 0.$$
(B2)

We define a generating function $H_I(z) = \sum_{O=0}^{\infty} z^O \mathcal{P}(I, O)$. By multiplying Eq. (B2) by z^O and then summing over O, we derive the following equation for $H_I(z)$:

$$\gamma_{I}[(I+1)H_{I+1}(z) - IH_{I}(z)] + F[H_{I-1}(z) - H_{I}(z)] + \gamma_{O}(1-z)H_{I}'(z) + R(I)(z-1)H_{I}(z) = 0.$$
(B3)

Plugging in z = 1, Eq. (B3) can be solved for $H_I(1) = \mathcal{P}(I)$, the marginal probability distribution of the input. The result is $\mathcal{P}(I) = (F/\gamma_I)^I \exp(-F/\gamma_I)/I!$,

the Poisson distribution. This implies that the first and second input moments are given by

$$\langle I \rangle = \frac{F}{\gamma_I} \equiv \overline{I}, \qquad \langle I^2 \rangle = \frac{F^2}{\gamma_I^2} + \frac{F}{\gamma_I} = \overline{I}^2 + \overline{I}.$$
 (B4)

Moments involving the output O can be obtained by manipulation of Eq. (B3). Taking its first derivative with respect to z, and then setting z = 1, we find

$$\gamma_{I}[(I+1)H'_{I+1}(1) - IH'_{I}(1)] + F[H'_{I-1}(1) - H'_{I}(1)] - \gamma_{O}H'_{I}(1) + R(I)H_{I}(1) = 0.$$
(B5)

Similarly, taking the second derivative of Eq. (B3) with respect to z, and setting z = 1, gives

$$\gamma_{I}[(I+1)H_{I+1}''(1) - IH_{I}''(1)] + F[H_{I-1}''(1) - H_{I}''(1)] - 2\gamma_{O}H_{I}''(1) + 2R(I)H_{I}'(1) = 0.$$
(B6)

From the definition of the generating function, $H'_I(1) = \sum_{O=0}^{\infty} O\mathcal{P}(I, O)$ and $H''_I(1) = \sum_{O=0}^{\infty} O(O-1)\mathcal{P}(I, O)$. Summing Eqs. (B5) and (B6) over all *I* yields the following moment relations:

$$\sum_{I=0}^{\infty} H_I'(1) = \gamma_O^{-1} \sum_{I=0}^{\infty} R(I) H_I(1)$$

$$\Rightarrow \langle O \rangle = \gamma_O^{-1} \langle R(I) \rangle,$$

$$\sum_{I=0}^{\infty} H_I''(1) = \gamma_O^{-1} \sum_{I=0}^{\infty} R(I) H_I'(1)$$

$$\Rightarrow \langle O^2 \rangle - \langle O \rangle = \gamma_O^{-1} \langle OR(I) \rangle. \quad (B7)$$

Evaluating $\langle O \rangle$ involves finding the mean of R(I) over the known input distribution $H_I(1) = \mathcal{P}(I)$. However, finding $\langle O^2 \rangle$ involves the unknown distribution $H'_I(1)$. Moreover, the last remaining moment in Eq. (B1) for the mean-squared error, $\langle OI \rangle$, can also be expressed in terms of this distribution, $\langle OI \rangle = \sum_{I=0}^{\infty} IH'_I(1)$. Thus, it is crucial to have additional information about $H'_I(1)$.

We know that $H'_{I}(1)$ satisfies Eq. (B5), and we assume an ansatz for $H'_{I}(1)$ of the form $H'_{I}(1) = \gamma_{O}^{-1}H_{I}(1)G(I)$ for some function G(I). Plugging this into Eq. (B5), and using the fact that $H_{I}(1)$ is the Poisson distribution, we find

$$H_I(1)[(S-1)G(I) + R(I)] = 0,$$
(B8)

where S is an operator acting on G(I), defined as

$$\mathcal{S} = \gamma_O^{-1}(\gamma_I I \Delta_{-1} + F \Delta_1). \tag{B9}$$

Here, Δ_h is the finite difference operator, which acts on a function f(I) as $\Delta_h f(I) \equiv f(I+h) - f(I)$. Thus, the

function G(I) that solves Eq. (B8) is $G(I) = (1 - S)^{-1}$ $R(I) \equiv \mathcal{L}R(I)$, where the operator $\mathcal{L} = \sum_{n=0}^{\infty} S^n$. Thus, $H'_I(1) = \gamma_O^{-1} H_I(1) \mathcal{L}R(I)$, and

$$\langle OI \rangle = \gamma_O^{-1} \langle I \mathcal{L} R(I) \rangle, \qquad \langle OR(I) \rangle = \gamma_O^{-1} \langle R(I) \mathcal{L} R(I) \rangle.$$

(B10)

Note that the terms on the right-hand sides inside the $\langle \rangle$ brackets are solely functions of *I*, and hence, the averages depend on $\mathcal{P}(I)$. Plugging Eqs. (B4), (B7), and (B10) into Eq. (B1) gives an expression for the relative error:

$$E = 1 - \frac{\bar{I}^{-1} \langle (I\mathcal{L} - \bar{I})R(I) \rangle^2}{\gamma_O \langle R(I) \rangle + \mathcal{M}[R(I)]},$$
$$\mathcal{M}[R(I)] \equiv \langle R(I)\mathcal{L}R(I) \rangle - \langle R(I) \rangle^2.$$
(B11)

To make further progress on the evaluation of E, it would be helpful to express R(I) in terms of eigenfunctions of S(which would also be eigenfunctions of \mathcal{L}). To do this, we employ a set of techniques known as umbral calculus [20], which starts with the observation that the function R(I) can be expanded in a Newton series (the finite difference analog of the Taylor series),

$$R(I) = \sum_{m=0}^{\infty} \rho_m(I)_m, \qquad \rho_m \equiv \frac{1}{m!} \Delta_1^m R(I)|_{I=0}, \quad (B12)$$

where $(I)_m \equiv I(I-1)...(I-m+1) = m!\binom{I}{m}$ is the *m*th falling factorial of *I* [with $(I)_0 \equiv 1$]. The Newton series expansion exists assuming R(I) fulfills certain analyticity and growth conditions [31], which are satisfied for all physically realistic production functions. Finite difference operators acting on $(I)_m$ result in linear combinations of falling factorials. In particular, $\Delta_1(I)_m = m(I)_{m-1}$ and $I\Delta_{-1}(I)_m = -m(I)_m$. Thus, the operator *S* acting on $(I)_m$ gives

$$\mathcal{S}(I)_m = -\frac{m\gamma_I}{\gamma_O}[(I)_m - \bar{I}(I)_{m-1}]. \tag{B13}$$

If we consider functions like R(I) as vectors in the basis of falling factorials $\{(I)_m, m = 0, 1, ...\}$, with components ρ_m , then from Eq. (B13) the operator S is a simple bidiagonal matrix in this basis, with elements

$$S_{m',m} = -\frac{m\gamma_I}{\gamma_O}\delta_{m',m} + \frac{m\gamma_I\overline{I}}{\gamma_O}\delta_{m',m-1}.$$
 (B14)

The eigenvalues of λ_n of S, labeled by n = 0, 1, ... in decreasing order, are just the diagonal matrix components, $\lambda_n = -n\gamma_I/\gamma_O$. The corresponding eigenfunctions are

$$v_n(I) = \sum_{m=0}^n \binom{n}{m} (-\bar{I})^m (I)_{n-m}.$$
 (B15)

The *n*th eigenfunction $v_n(I)$ is a polynomial in *I* of degree *n*, with the first few eigenfunctions given by

$$v_0(I) = 1,$$
 $v_1(I) = I - \overline{I},$ $v_2(I) = (I - \overline{I})^2 - I,$
 $v_3(I) = (I - \overline{I})^3 - 3I(I - \overline{I}) + 2I.$ (B16)

The eigenfunctions $v_n(I)$ are mathematically related to expansions of the master equation through alternative approaches, for example, the spectral method of Refs. [25,26]. In fact, $v_n(I) = n! \langle n|I \rangle$, where $\langle n|I \rangle$ is the mixed product defined in Eq. (A8) of Ref. [25] (with \overline{I} substituted for the rate parameter g).

Since Eq. (B15) can be inverted to express $(I)_m$ in terms of the eigenfunctions,

$$(I)_m = \sum_{n=0}^m \binom{m}{n} \bar{I}^{m-n} v_n(I), \qquad (B17)$$

we can write R(I) in terms of the eigenfunctions by plugging Eq. (B17) into Eq. (B12),

$$R(I) = \sum_{n=0}^{\infty} \sigma_n v_n(I), \quad \sigma_n \equiv \sum_{m=0}^{\infty} \binom{m}{n} \rho_m \bar{I}^{m-n}, \quad (B18)$$

where we use the property that $\binom{m}{n} = 0$ for n > m. The operator $\mathcal{L} = \sum_{k=0}^{\infty} S^k$ acting on R(I) is then

$$\mathcal{L}R(I) = \sum_{n=0}^{\infty} \sigma_n \sum_{k=0}^{\infty} \left(-\frac{n\gamma_I}{\gamma_O} \right)^k v_n(I)$$
$$= \sum_{n=0}^{\infty} \sigma_n \frac{\gamma_O}{\gamma_O + n\gamma_I} v_n(I).$$
(B19)

Since the quantities in Eq. (B11) for *E* involve averages with respect to $\mathcal{P}(I)$, it is useful to derive the first and second moments of the eigenfunctions. From the fact that the falling factorials have very simple averages in the Poisson distribution, $\langle (I)_m \rangle = \overline{I}^m$, we find using Eq. (B15) that $\langle v_n(I) \rangle = \delta_{n,0}$. This implies that $\langle R(I) \rangle =$ $\langle \mathcal{L}R(I) \rangle = \sigma_0$. To find $\langle v_{n'}(I)v_n(I) \rangle$, we start from the Chu-Vandermonde identity [20], the umbral analog of the binomial theorem,

$$(x+y)_m = \sum_{k=0}^m \binom{m}{k} (x)_{m-k} (y)_k.$$
 (B20)

For x = I - m' and y = m', this gives

$$(I)_{m} = \sum_{k=0}^{n} \binom{m}{k} (I - m')_{m-k} (m')_{k}$$
$$= \sum_{k=0}^{n} k! \binom{m}{k} \binom{m'}{k} (I - m')_{m-k}, \quad (B21)$$

where we use the fact that $(m)_k = k! \binom{m}{k}$. Multiplying both sides by $(I)_{m'}$, we find

$$(I)_{m'}(I)_m = \sum_{k=0}^n k! \binom{m}{k} \binom{m'}{k} (I)_{m'}(I-m')_{m-k}$$
$$= \sum_{k=0}^n k! \binom{m}{k} \binom{m'}{k} (I)_{m+m'-k}.$$
(B22)

The second equality is based on the relation $(I)_{i+j} = (I)_i(I-i)_j$, which follows from the definition of the falling factorial. Taking the average of both sides of Eq. (B22) yields

$$\langle (I)_{m'}(I)_m \rangle = \sum_{k=0}^n k! \binom{m}{k} \binom{m'}{k} \bar{I}^{m+m'-k}.$$
 (B23)

An alternative expression for $\langle (I)_{m'}(I)_m \rangle$ can be derived by substituting the eigenfunction expansion of Eq. (B17) for both $(I)_{m'}$ and $(I)_m$,

$$\langle (I)_{m'}(I)_{m} \rangle = \sum_{n'=0}^{m'} \sum_{n=0}^{m} \binom{m'}{n'} \binom{m}{n} \bar{I}^{m+m'-n-n'} \langle v_{n'}(I) v_{n}(I) \rangle.$$
(B24)

Comparing the right-hand sides of Eqs. (B23) and (B24), we see that $\langle v_{n'}(I)v_n(I)\rangle = n!\bar{I}^n\delta_{n',n}$. Together with Eqs. (B18) and (B19), this allows us to calculate

$$\mathcal{M}[R(I)] = \langle R(I)\mathcal{L}R(I) \rangle - \langle R(I) \rangle^{2}$$

= $\sum_{n'=0}^{\infty} \sum_{n=0}^{\infty} \sigma_{n'} \sigma_{n} \frac{\gamma_{O}}{\gamma_{O} + n\gamma_{I}} \langle v_{n'}(I)v_{n}(I) \rangle - \sigma_{0}^{2}$
= $\sum_{n=1}^{\infty} \sigma_{n}^{2} \frac{\gamma_{O} n! \overline{I}^{n}}{\gamma_{O} + n\gamma_{I}}.$ (B25)

Using the fact that $I = \overline{I}v_0(I) + v_1(I)$, we can similarly evaluate

$$\langle (I\mathcal{L} - \bar{I})R(I) \rangle$$

$$= \sum_{n=0}^{\infty} \sigma_n \left[\bar{I} \langle v_0(I)v_n(I) \rangle + \frac{\gamma_O}{\gamma_O + \gamma_I} \langle v_1(I)v_n(I) \rangle \right] - \bar{I}\sigma_0$$

$$= \frac{\gamma_O \bar{I}\sigma_1}{\gamma_O + \gamma_I}.$$
(B26)

Plugging Eqs. (B25) and (B26) into Eq. (B11), we obtain our final expression for the relative error:

$$E = 1 - \frac{\bar{I}\gamma_O^2 \sigma_1^2}{(\gamma_I + \gamma_O)^2} \left[\gamma_O \sigma_0 + \sum_{n=1}^{\infty} \sigma_n^2 \frac{\gamma_O n! \bar{I}^n}{\gamma_O + n\gamma_I} \right]^{-1}.$$
 (B27)

This expression can be readily calculated numerically for any given R(I), as was done in the main text for the family of Hill function production rates. To facilitate evaluation, we express the coefficients σ_n as moments with respect to the Poisson distribution $\mathcal{P}(I)$ in the following manner, using the expansion of Eq. (B18):

$$\langle v_n(I)R(I)\rangle = \sum_{n'=0}^{\infty} \sigma_{n'} \langle v_{n'}(I)v_n(I)\rangle = \sigma_n n! \overline{I}^n$$

$$\Rightarrow \sigma_n = \frac{\langle v_n(I)R(I)\rangle}{n! \overline{I}^n}.$$
(B28)

From the definition of $v_n(I)$ in Eq. (B15), the coefficients σ_n can be written:

$$\sigma_n = \sum_{m=0}^n \frac{(-1)^{n-m} \bar{I}^{-m}}{(n-m)!} \left\langle \begin{pmatrix} I \\ m \end{pmatrix} R(I) \right\rangle.$$
(B29)

Using Eq. (B29), the σ_n can be numerically calculated for any R(I). The sum in Eq. (B27) converges quickly because the σ_n decrease rapidly with n, so typically, only σ_n for $n \le 5$ are needed to get accurate results for E.

The expression in Eq. (B27) also allows us to determine under what conditions the relative error E becomes minimal. For this to occur, we need $\sigma_1 \neq 0$, since otherwise, E takes its maximum value of 1. The sum within the brackets in Eq. (B27) is composed of only non-negative terms, and E is smallest when this sum is minimal. This can be achieved by setting $\sigma_n = 0$ for all $n \ge 2$. Thus, E is bounded from below by

$$E \ge 1 - \frac{\bar{I}\gamma_O^2 \sigma_1^2}{(\gamma_I + \gamma_O)^2} \left[\gamma_O \sigma_0 + \sigma_1^2 \frac{\gamma_O \bar{I}}{\gamma_O + \gamma_I} \right]^{-1}, \quad (B30)$$

where the equality is reached only when R(I) has an optimal linear form, $R_{opt}(I) = \sigma_0 v_0(I) + \sigma_1 v_1(I) = \sigma_0 + \sigma_1(I - \overline{I})$. The right-hand side of Eq. (B30) is minimized with respect to γ_O when $\gamma_O = \gamma_I \sqrt{1 + \tilde{\Lambda}}$, with $\tilde{\Lambda} \equiv \overline{I} \sigma_1^2 / \sigma_0 \gamma_I$. At this optimal γ_O , the inequality in Eq. (B30) becomes

$$E \ge \frac{2}{1 + \sqrt{1 + \tilde{\Lambda}}} \equiv E_{\text{opt}}.$$
 (B31)

APPENDIX C: MAPPING THE ENZYMATIC PUSH-PULL LOOP ONTO THE WK FILTER

The full set of reactions for the enzymatic push-pull loop is given by

The corresponding steady-state populations are

$$\bar{K} = \frac{F}{\gamma_K}, \quad \bar{S}_K = \frac{F\kappa_+}{\gamma_K\kappa_-}, \quad \bar{S}^* = \frac{F\kappa_r\kappa_+\rho_-}{\gamma_K\kappa_-\rho_r\rho_+}, \quad \bar{S}_P^* = \frac{F\kappa_r\kappa_+}{\gamma_K\kappa_-\rho_r},$$
(C2)

where $\kappa_{+} = \kappa_{b}\bar{S}$, $\kappa_{-} = \kappa_{u} + \kappa_{r}$, $\kappa = \kappa_{+} + \kappa_{-}$, $\rho_{+} = \rho_{b}\bar{P}$, $\rho_{-} = \rho_{u} + \rho_{r}$, and $\rho = \rho_{+} + \rho_{-}$.

For the system in Eq. (C1), the associated set of chemical Langevin equations is

$$\frac{dK}{dt} = F - \gamma_K K - \kappa_b KS + (\kappa_u + \kappa_r)S_K + n_1 + n_2 + n_3,
\frac{dS_K}{dt} = \kappa_b KS - (\kappa_u + \kappa_r)S_K - n_2 - n_3,
\frac{dS^*}{dt} = \kappa_r S_K - \rho_b PS^* + \rho_u S_P^* + n_3 + n_4,
\frac{dS_P^*}{dt} = \rho_b PS^* - (\rho_u + \rho_r)S_P^* - n_4 + n_5,
\frac{dP}{dt} = -\frac{dS_P^*}{dt}, \qquad \frac{dS}{dt} = -\frac{dS_K}{dt} - \frac{dS^*}{dt} - \frac{dS_P^*}{dt}, \quad (C3)$$

where the equations on the last line come from the assumptions that the total populations of free or bound phosphatase $(P + S_P^*)$ and free or bound substrate in all its forms $(S + S_K + S^* + S_P^*)$ remain constant. The noise terms $n_i(t) = \sqrt{P_{n_i}}\eta_i(t)$, where the $\eta_i(t)$ are Gaussian white noise functions with correlations $\langle \eta_i(t)\eta_j(t')\rangle = \delta_{ij}\delta(t-t')$. The constants P_{n_i} are the power spectra of the noise terms, given by

$$P_1 = 2\gamma_K \bar{K}, \qquad P_2 = \kappa_b \bar{K} \bar{S} + \kappa_u \bar{S}_K, \qquad P_3 = \kappa_r \bar{S}_K,$$

$$P_4 = \rho_b \bar{P} \bar{S}^* + \rho_u \bar{S}_P^*, \qquad P_5 = \rho_r \bar{S}_P^*. \qquad (C4)$$

We are interested in how the kinase input signal $\delta I = \delta K + \delta S_K$ is transduced into the active substrate output $\delta O = \delta S^* + \delta S_P^*$, and, in particular, whether the system can be approximately mapped onto a WK noise filter of the form given in the main text [Eq. (2)]. [Recall that $\delta x(t) \equiv x(t) - \bar{x}$ for any time series x(t).] Since the WK description

hinges on the form of the correlation functions of input and output, we need to calculate such correlations for the dynamical equations in Eq. (C3). After linearizing these equations, it will be easier to work in Fourier space, where the Fourier-transformed correlation functions correspond to power spectra: $P_{\delta x}(\omega) = \int dt \langle \delta x(t) \delta x(0) \rangle e^{i\omega t}$ for a given $\delta x(t)$. Hence, it will useful, before proceeding further, to recast Eq. (2), the time-domain noise filter, as a Fourierspace relation in terms of the power spectra. The result is

$$P_{\delta I}(\omega) = \frac{2F\gamma_I^{-2}}{1 + (\omega/\gamma_I)^2},$$

$$P_{\delta O}(\omega) = \frac{(R_1/\gamma_O G)^2}{1 + (\omega/\gamma_O)^2} \left[G^2 P_{\delta I}(\omega) + \frac{2F(G/\gamma_I)^2}{\Lambda} \right]. \quad (C5)$$

Our goal in this section is to show that $P_{\delta I}$ and $P_{\delta O}$ calculated for the enzymatic push-pull loop in Eq. (C3) have the approximate form of Eq. (C5), with effective values for γ_I , γ_O , R_1 , and Λ expressed in terms of the loop reaction rate parameters.

The equilibrium populations \bar{K} and \bar{S}_K scale with \bar{I} as $\bar{K} = (\kappa_-/\kappa)\bar{I}$ and $\bar{S}_K = (\kappa_+/\kappa)\bar{I}$. Similarly, $\bar{S}^* = (\rho_-/\rho)\bar{O}$ and $\bar{S}_P^* = (\rho_+/\rho)\bar{O}$. Each deviation from the mean— δK , δS_K , δS^* , and δS_P^* —we explicitly divide into a component that scales with δI or δO like the mean population (the "slowly" varying component), and the remainder (the "quickly" varying component, denoted with subscript q):

$$\delta K = \frac{\kappa_{-}}{\kappa} \delta I + \delta I_{q}, \qquad \delta S_{K} = \frac{\kappa_{+}}{\kappa} \delta I - \delta I_{q},$$

$$\delta S^{*} = \frac{\rho_{-}}{\rho} \delta O + \delta O_{q}, \qquad \delta S_{P}^{*} = \frac{\rho_{+}}{\rho} \delta O - \delta O_{q}. \quad (C6)$$

We can interpret Eq. (C6) as defining a change of variables from the set δK , δS_K , δS^* , δS_P^* to the set δO , δO_q , δI , δI_q . The nomenclature of slow and quick components comes from the fact that if the enzymatic reaction rates ($\kappa_+, \kappa_-, \rho_+, \rho_-$) are made extremely rapid, the characteristic time scales for the δI_q and δO_q fluctuations become so small that the quick components can be neglected, since there would be nearly instantaneous equilibration between the free and bound enzyme populations. In general, however, we cannot assume this limiting case always holds, so we take into account both the slow and quick components in our analysis.

The dynamical system of Eq. (C3), after linearization, Fourier transform, and the change of variables in Eq. (C6), takes the form of a linear system of equations that can be written in matrix form as

$$\begin{pmatrix} -i\omega + \frac{\kappa_{-Y_{K}}}{\kappa_{+}} & \gamma_{K} & 0 & 0\\ \frac{\kappa_{+}(i\omega\bar{S}-\kappa_{+}\bar{K})}{\kappa\bar{S}} & -i\omega + \kappa + \frac{\kappa_{+}\bar{K}}{\bar{S}} & -\frac{\kappa_{+}\bar{K}}{\bar{S}} & 0\\ -\frac{\kappa_{r}\kappa_{+}}{\kappa} & \kappa_{r} & -i\omega + \frac{\rho_{r}\rho_{+}}{\rho} & -\rho_{r}\\ 0 & 0 & \frac{\rho_{+}(i\omega\bar{P}-\rho_{+}\bar{S}^{*})}{\rho\bar{P}} & -i\omega + \rho + \frac{\rho_{+}\bar{S}^{*}}{\bar{P}} \end{pmatrix} \\ \times \begin{pmatrix} \delta \tilde{I} \\ \delta \tilde{O} \\ \delta \tilde{O} \\ \delta \tilde{O} \\ \delta \tilde{O} \\ \eta \end{pmatrix} = \begin{pmatrix} \tilde{n}_{1} \\ \tilde{n}_{2}+\tilde{n}_{3} \\ \tilde{n}_{3}+\tilde{n}_{5} \\ \tilde{n}_{4}-\tilde{n}_{5} \end{pmatrix},$$
(C7)

where $\tilde{x}(\omega)$ denotes the Fourier transform of x(t). Equation (C7) can be solved analytically for $\delta \tilde{O}$, $\delta \tilde{O}_q$, $\delta \tilde{I}$, $\delta \tilde{I}_q$, though for simplicity we do not write out the full solutions, since these would take up too much space. Rather, we sketch out the basic approach to calculating and approximating the associated power spectra. The structure of the solutions to Eq. (C7), for example, $\delta \tilde{I}$, is a linear combination of the noise functions, $\delta \tilde{I}(\omega) = \sum_{i=1}^{5} a_{\delta I,i}(\omega)\tilde{n}_i(\omega)$, with coefficients $a_{\delta I,i}(\omega)$. The corresponding power spectrum is $P_{\delta I}(\omega) = \sum_{i=1}^{5} |a_{\delta I,i}(\omega)|^2 P_{n_i}$, with P_{n_i} given by Eq. (C4). The function $P_{\delta I}(\omega)$ can be written out in the form of a rational function with even powers of ω in the numerator and denominator,

$$P_{\delta I}(\omega) = \frac{\sum_{i=0}^{N} n_{\delta I,i} \omega^{2i}}{1 + \sum_{i=1}^{D} d_{\delta I,i} \omega^{2i}},$$
(C8)

where $n_{\delta I,i}$ and $d_{\delta I,i}$ are coefficients independent of ω , and N = 3, D = 4 for the case of $P_{\delta I}$. In order to simplify

Eq. (C8) further, we make two assumptions. (i) The characteristic time scale over which the input signal varies, γ_K^{-1} , is much longer than the characteristic time scales of the enzymatic reactions, κ_a^{-1} and ρ_a^{-1} , where α denotes the various subscripts +, -, and *r*. For the parameters in the main text, $\gamma_K^{-1} \sim \mathcal{O}(10^2 \text{ s})$, while κ_a^{-1} , $\rho_a^{-1} \sim \mathcal{O}(10^{-1}-10^0 \text{ s})$. This is the physically interesting regime, since we can expect the system to efficiently transduce signals that vary more slowly than the intrinsic reactions that carry out the transduction. Limiting our focus to frequencies $\omega \ll \kappa_a^{-1}$, ρ_a^{-1} , it turns out that the higher-order powers of ω in both the numerator and denominator of Eq. (C8) are negligible, and the power spectrum can be approximated by

$$P_{\delta I}(\omega) \approx \frac{n_{\delta I,0}}{1 + d_{\delta I,1}\omega^2}.$$
 (C9)

(ii) We assume that the system is in the regime where $\bar{K} = F/\gamma_K \ll \bar{S}$, \bar{P} . Thus, we expand the coefficients $n_{\delta I,0}$ and $d_{\delta I,1}$ in Eq. (C9) up to first order in \bar{K}/\bar{S} and \bar{K}/\bar{P} , resulting in a $P_{\delta I}(\omega)$ that has the form of Eq. (C5). Namely, $n_{\delta I,0} \approx 2F\gamma_I^{-2}$ and $d_{\delta I,1} \approx \gamma_I^{-2}$, where the effective γ_I^{-2} is given by

$$\gamma_I = \frac{\kappa_- \gamma_K}{\kappa} + \frac{\kappa_+^2 (\rho_r \rho_+ + \kappa_r \rho) \gamma_K \bar{K}}{\kappa^2 \rho_r \rho_+ \bar{S}}.$$
 (C10)

In an analogous manner, we can find the correspondence between $P_{\delta O}(\omega)$ and the form in Eq. (C5), leading to the following expressions for the remaining effective parameters:

$$\begin{split} \gamma_{O} &= \frac{\rho_{r}\rho_{+}}{\sqrt{\rho^{2} - 2\rho_{r}\rho_{+}}} - \frac{\kappa_{r}\kappa_{+}\rho_{+}\rho_{-}\rho\bar{K}}{\kappa_{-}(\rho^{2} - 2\rho_{r}\rho_{+})^{3/2}\bar{P}}, \qquad R_{1} = \frac{\kappa_{r}\kappa_{+}\rho}{\kappa\sqrt{\rho^{2} - 2\rho_{r}\rho_{+}}} - \frac{2\kappa_{r}^{2}\kappa_{+}^{2}\rho_{+}\rho_{-}\bar{K}}{\kappa_{-}\kappa(\rho^{2} - 2\rho_{r}\rho_{+})^{3/2}\bar{P}}, \\ \Lambda &= \frac{\kappa_{r}\kappa_{+}\kappa^{2}\rho^{2}}{\gamma_{K}\kappa_{-}[\rho^{2}(\kappa^{2} - \kappa_{r}\kappa_{+}) - \rho_{r}\rho_{+}\kappa^{2}]} + \frac{\kappa_{r}\kappa_{+}^{2}\kappa\rho\bar{K}}{\gamma_{K}\rho_{r}\kappa_{-}^{2}\rho_{+}[\rho^{2}(\kappa_{r}\kappa_{+} - \kappa^{2}) + \rho_{r}\kappa^{2}\rho_{+}]^{2}\bar{S}\bar{P}}[(\kappa_{r}^{2}\kappa_{+}\rho^{3}(\kappa_{+} - \kappa_{-}) \\ +\kappa_{r}\rho\{\rho_{r}\rho_{+}[2\kappa_{+}^{3} + \kappa_{+}^{2}(2\kappa_{-} + \rho) - 2\kappa_{+}\kappa_{-}^{2} + \kappa_{-}^{2}(\rho - 2\kappa_{-})] - 2\kappa^{2}\rho^{2}(\kappa_{+} - \kappa_{-})\} \\ &+ 2\rho_{r}\kappa_{+}\kappa^{2}\rho_{+}(\rho_{r}\rho_{+} - \rho^{2}))\rho\bar{P} + \kappa_{r}\rho_{r}\kappa^{3}\rho_{+}\rho_{-}(\rho_{-} - \rho_{+})\bar{S}]. \end{split}$$
(C11)

The results in Eqs. (C10) and (C11), without the first-order corrections in \bar{K}/\bar{S} and \bar{K}/\bar{P} , correspond to Eq. (8) in the main text.

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